### **KNEE**

# Patient-specific instrumentation improved mechanical alignment, while early clinical outcome was comparable to conventional instrumentation in TKA

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#### Abstract

*Purpose* The aim of this prospective study was to compare early clinical outcome, radiological limb alignment, and three-dimensional (3D)-component positioning between conventional and computed tomography (CT)based patient-specific instrumentation (PSI) in primary mobile-bearing total knee arthroplasty (TKA).

*Methods* Two hundred ninety consecutive patients (300 knees) with severe, debilitating osteoarthritis scheduled for TKA were included in this study using either conventional instrumentation (CVI, n = 150) or PSI (n = 150). Patients were clinically assessed before and 2 years after surgery according to the Knee-Society-Score (KSS) and the visual-analog-scale for pain (VAS). Additionally, the Western Ontario McMaster Universities Osteoarthritis Index (WOMAC) and the Oxford-Knee-Score (OKS) were collected at follow-up. To evaluate accuracy of CVI and PSI, hip-knee-ankle angle (HKA) and 3D-component positioning were assessed on postoperative radiographs and CT.

*Results* Data of 222 knees (CVI: n = 108, PSI: n = 114) were available for analysis after a mean follow-up of 28.6  $\pm$  5.2 months. At the early follow-up, clinical outcome (KSS, VAS, WOMAC, OKS) was comparable between the

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Department of Orthopedics, St. Vincent Hospital, Stumpergasse 13, 1060 Vienna, Austria e-mail: werner.anderl@bhs.at two groups. Mean HKA-deviation from the targeted neutral mechanical axis (CVI:  $2.2^{\circ} \pm 1.7^{\circ}$ ; PSI:  $1.5^{\circ} \pm 1.4^{\circ}$ ; p < 0.001), rates of outliers (CVI: 22.2 %; PSI: 9.6 %; p = 0.016), and 3D-component positioning outliers were significantly lower in the PSI group. Non-outliers (HKA:  $180^{\circ} \pm 3^{\circ}$ ) showed better clinical results than outliers at the 2-year follow-up.

*Conclusions* CT-based PSI compared with CVI improves accuracy of mechanical alignment restoration and 3D-component positioning in primary TKA. While clinical outcome was comparable between the two instrumentation groups at early follow-up, significantly inferior outcome was detected in the subgroup of HKA-outliers.

*Level of evidence* Prospective comparative study, Level II.

**Keywords** Patient-specific instrumentation  $\cdot$  Total knee arthroplasty  $\cdot$  MyKnee  $\cdot$  CT-based cutting block  $\cdot$  Clinical and radiological outcome  $\cdot$  3D-component positioning

# Introduction

Neutral mechanical limb alignment and adequate component positioning are primary intra-operative goals thought to be essential for satisfactory long-term outcome after total knee arthroplasty (TKA) [17, 24, 49]. Various studies showed that coronal limb alignment is an important factor in implant durability as outliers in the frontal plane had a significantly higher risk for early loosening and polyethylene wear with decreased overall implant survival [17, 49]. Mechanical malalignment and component malpositioning have also been identified as influencing factors for unsatisfactory clinical outcome [3, 34]. Although the impact of neutral mechanical alignment on implant longevity is still a

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matter of discussion, there is currently no better parameter to aim for when performing TKA [7, 32, 46].

Despite adequate surgical technique, improvements, and simplifications in manual instrumentation systems, malalignment remains a common issue in conventional TKA [10, 14]. A contemporary method to potentially optimize accuracy of alignment in TKA is the use of patient-specific instrumentation (PSI). For patient-specific methods, computed tomography scans (CT) or magnetic resonance images (MRI) are used for preoperative planning and production of patientmatched pin guides or cutting blocks. Early investigations were predominantly reporting on patient-matched systems based on preoperative MRI [2, 4, 8, 9, 11, 22, 40-45, 48, 61, 64, 67], while recently more authors reported on CTbased systems [5, 13, 16, 20, 26, 29, 30, 50, 61, 66]. However, providing a unique fit on the distal femur and proximal tibia, these jigs are used for exact bone resection and component positioning. Potential benefits, such as reduced surgical time and increased accuracy of TKA, come at the cost of increased economic and logistic expenses. Thus, there is great scientific and practical interest in the actual advantages and reliability of these systems [4, 43, 55-57].

At present, there is no consensus in literature regarding accuracy and reliability of patient-matched instrumentation as current studies showed controversial and inconsistent radiological results of various PSI systems; while some authors reported improved alignment and component positioning [2, 14, 22, 26, 40–42, 45], others described comparable [9, 20, 50] or unsatisfactory results [1, 8, 11, 18, 35, 44, 51, 52, 63, 66, 67].

Despite increasing numbers of reports regarding radiological results with PSI systems, investigations focusing on or additionally addressing clinical outcome are scarce, and currently, they are limited by short follow-up periods and small sample sizes [1, 47, 48, 64, 66, 67]. Since the impact of radiological alignment is still controversial and clinical results with PSI are not often reported, clinical combined with radiological assessment becomes more relevant.

Thus, the purpose of the present study was to compare clinical results, as well as radiological limb alignment, and three-dimensional (3D)-component positioning between conventional instrumentation (CVI) and a CT-based PSI in primary mobile-bearing TKA. We hypothesized that (a) clinical outcome would be comparable between PSI and CVI and (b) PSI would be superior regarding mechanical alignment restoration, number of outliers, and 3D-component positioning compared with CVI.

# Materials and methods

Included were all patients, regardless of preoperative varus or valgus deformity, scheduled for primary TKA with a mobile-bearing TKA system (GMK<sup>®</sup> Primary, Medacta International S.A., Castel San Pietro, Switzerland). Initially, the aim of the present single-center study was to evaluate this new TKA system using standard instrumentation regarding clinical outcome, accuracy and reliability of 3D-component positioning, and mechanical alignment restoration. However, in 2010, a PSI method (MyKnee<sup>®</sup>, Medacta International S.A., Castel San Pietro, Switzerland) for the same mobile-bearing TKA system was introduced and became the preferred method for performing TKA at our institution. Consequently, we expanded the aim of our study toward a comparison between the two methods of instrumentation, to determine additional benefits of the patient-specific method. The same protocol was used for both study groups.

Between January 2007 and September 2011, patients with osteoarthritis of the knee joint (Kellgren–Lawrence [28] grading II, III, or IV) scheduled for TKA at our institution were assessed for their eligibility as study participants. The first 150 cases of each group meeting the inclusion criteria were enrolled in the study. Criteria for exclusion were previous open surgeries of the knee joint, major trauma or debilitating comorbidities influencing mobility, inability to complete the questionnaire due to cognitive difficulties, and patient refusal for participation. Informed consent was provided by all included patients. A flow chart of patient enrollment is presented in Fig. 1.

Preoperative PSI workflow and surgical technique

Preoperative CT scans according to the standardized MyKnee<sup>®</sup> protocol (Medacta International S.A., Castel San Pietro, Switzerland) were taken. Cutting blocks and 3D bone models of the knee were produced according to the preferences of the surgeon aiming for a postoperative neutral mechanical axis, a physiological joint line, an anatomical tibial slope (0° to 6° depending on the preoperative condition), and a flush fitting of the femoral component to avoid anterior notching (0° to 4° flexion), together with a femoral component rotation parallel to the transepicondylar axis.

All patients underwent implantation of a standard mobile-bearing total knee prosthesis (GMK<sup>®</sup> Primary, Medacta International S.A., Castel San Pietro, Switzerland) without patella resurfacing. After a midline skin incision, followed by a medial or lateral parapatellar approach, bone cuts were performed in the CVI group using the standard GMK<sup>®</sup> instrumentation system assisted by an extra-medullary guidance rod for the tibia and an intra-medullary guidance rod for the femur and spacer blocks. In PSI, the tibial and femoral footprint areas were carefully cleaned of the remaining cartilage for an exact fit of the cutting blocks, and after pinning, bone cuts were performed in accordance to the preoperative planning. Tibial rotation was determined



Fig. 1 Flowchart of patient enrollment

clinically according to bony structures in both groups. Fixation of components was either cemented or cementless. Ligament balancing and removal of osteophytes were performed carefully in both groups. Four senior orthopedic surgeons experienced in TKA performed all surgeries, each with both techniques. Postoperative treatment was the same in both groups with respect to pain relief and mobilization.

# Clinical assessment

Preoperative data and data collected at a minimum of 2 years after surgery were evaluated. Patient characteristics such as age, gender, body mass index (BMI) were recorded. Clinical assessment included the Knee-Society-Score (KSS) [25] comprised of its two subscales: knee- and function-score. The range of motion (ROM) was recorded. The subjective knee questionnaire included a visual analog scale (VAS) for pain, the Western Ontario and McMaster Universities Osteoarthritis Index (WOMAC) [6, 53, 54], and the Oxford-Knee-Score (OKS) [15, 39]. All clinical follow-ups were performed by the same independent examiners (L.P., R.K., G.K., G.B.), who were blinded regarding the used method of instrumentation.

## Radiological assessment

In both groups, long-leg, anterior-posterior, lateral of the knee joint, and tangential patella radiographs were taken before surgery and before hospital discharge. In addition, patients of the PSI group underwent preoperative CT scans Fig. 2 Pre- (a) and postoperative (b, c, d) radiographic evaluations of hip-knee-ankle angle (HKA) and postoperative frontal femoral (FFC) and tibial (TFC) component angle on long-leg weight-bearing radiographs. Evaluation of lateral femoral (LFC) and tibial (LTC) component angle on sagittal short view radiographs. Femoral component rotation (FCR) measured on CT scans of the knee



at a minimum of 4 weeks before scheduled surgery according to the standardized MyKnee<sup>®</sup> protocol for planning and production of the individual cutting blocks.

For frontal mechanical alignment, the hip-knee-ankle angle (HKA) was measured on long-leg radiographs. Frontal femoral component (FFC) position was defined as the angle between the femoral mechanical axis and the tangent formed by the distal femoral condyles. Frontal tibial component (FTC) position was measured as the angle between the mechanical axis and the tibial plateau. Lateral component position was defined as the angle between the femoral or tibial axis and the respective implant surfaces (lateral femoral component angle, LFC; lateral tibial component angle, LTC). Femoral component rotation (FCR) was assessed on postoperative CTs of the first 25 patients of each group to limit radiation exposure and costs (Fig. 2).

Radiographic measurements were performed twice at two different time points by two independent examiners (L.P., G.B.). Intra- and inter-rater comparisons revealed measurement errors less than one degree for all examined parameters.

In order to analyze accuracy of mechanical axis restoration and 3D-component positioning between the CVI and PSI group, deviations from neutral mechanical alignment and targeted 3D-component positioning in degrees were calculated. Outliers were defined as deviations from the intra-operative goals (HKA 180° ± 3°, FFC 90° ± 2°, FTC 90° ± 2°, LFC [86° to 90°] ± 2°, LTC [84° to 90°] ± 2°, FCR 0°).

This trial was approved by the institutional review board and was carried out as a single-center study.

## Statistical analysis

A power analysis showed that a sample size of 100 knees per group is required to detect a mean difference of 10 points and an assumed standard deviation of 25 points in the KSS between the CVI and PSI group with a power of

Table 1         Group characteristics	Preoperative	CVI group $(n = 108)$	PSI group ( $n = 114$ )	p value
	Age* (years)	$67.7\pm9.6$	$68.7 \pm 8.2$	n.s.
<i>CVI</i> conventional instrumentation, <i>PSI</i> patient-specific instrumentation	Female/male <sup>†</sup> $(n)$	63/45	73/41	n.s.
	Body mass index* (kg/m <sup>2</sup> )	$29.8\pm5.4$	$29.9\pm5.2$	n.s.
	Right/left knee <sup>†</sup> ( $n$ )	57/51	60/54	n.s.
<ul> <li>* The values are given as the mean and the standard deviation</li> <li><sup>†</sup> The values are given as numbers</li> </ul>	Varus/valgus <sup>†</sup> $(n)$	81/27	89/25	n.s.
	Kellgren–Lawrence grading II/III/IV (n)	20/62/26	25/58/31	n.s.
	Mediolateral instability $\leq 5^{\circ}/6-9^{\circ}/\geq 10^{\circ}$ ( <i>n</i> )	30/11/1	30/5/1	n.s.

80 % at an  $\alpha$ -level of 0.05. To account for possible dropouts, we enrolled 150 knees in each group for a total of 300.

Descriptive statistic was used to present patients characteristics. Distribution of the data was assessed by a visual inspection of histograms and the Kolmogorov–Smirnov test. For normally distributed variables, the independent *t* test and the Mann–Whitney *U* test for nonparametric variables were used to compare differences in means between CVI and PSI, as well as between HKA-outliers and nonoutliers. Fisher's exact or chi-square tests were employed to examine the relationship between counts of binary variables and treatment groups. Statistical significance was reported at a *p* value of <0.05 level (two sided). All statistical analyses were performed in SPSS 21<sup>®</sup> (IBM<sup>®</sup> Corporation, Armonk, USA).

# Results

#### Demographics

Of 290 study participants (300 knees), 29 patients were lost to follow-up (follow-up rate 90 %), 39 patients were not included from analysis due to the following reasons: died during the follow-up period (n = 2), incomplete data (n = 17), debilitating comorbidities that developed during the follow-up period (n = 5), traumatic (periprosthetic) injuries of the operated leg or debilitating injuries to other body parts (n = 7), total joint arthroplasty of the opposite knee or other major orthopedic surgery within 6 months of follow-up (n = 6), severe postoperative contracture with consecutive mobilization (n = 4), and secondary patellar resurfacing (n = 3). Sub-analyses of baseline data including all group characteristics revealed no differences between cases included versus not included in analysis (Suppl. Table 1) and cemented versus cementless fixation (Suppl. Table 2). There was no necessity to intra-operatively abandon PSI in any case. Revision surgery for knee infection was indicated in two cases: for aseptic loosening of the tibia component in one case and for knee instability in the other case (Fig. 1).

A total of 222 knees (five patients underwent bilateral TKA) were followed for 28.6  $\pm$  5.2 months. The study cohort consisted of 108 cases in the CVI group and 114 cases in the PSI group. No significant differences in group characteristics were detected (Table 1).

# Clinical and radiological outcome

Clinical (KSS knee, KSS function, ROM, VAS) and radiological parameters (HKA, HKA of preoperative varus and valgus knees) improved significantly from pre- to postoperative in both groups (Tables 2, 3). At the early follow-up, clinical outcome was comparable between the two groups, whereas KSS function and VAS for pain were significantly better in the PSI group (Table 2). No significant differences between the CVI and PSI group were detected with the

 Table 2
 Clinical outcome between conventional (CVI) versus PSI after total knee arthroplasty

	CVI group $(n = 108)$	PSI group $(n = 114)$	p value
KSS knee (0–100 poi	ints)		
Preoperative	$44.3 \pm 18.6$	$42.8\pm23.3$	n.s.
2-Year follow-up	$92.7\pm10.7$	$92.2\pm11.8$	n.s.
p value	< 0.001	< 0.001	
KSS function (0-100	points)		
Preoperative	$53.1\pm22.6$	$47.4\pm26.5$	n.s.
2-Year follow-up	$80.9\pm20.4$	$86.8 \pm 16.3$	0.017
p value	< 0.001	< 0.001	
Range of motion (°)			
Preoperative	$109.6\pm16.2$	$110.9 \pm 16.4$	n.s.
2-Year follow-up	$116.6\pm12.1$	$116.9 \pm 11.8$	n.s.
p value	< 0.001	0.001	
VAS pain (0–10 poin	ets)		
Preoperative	$7.5 \pm 1.5$	$7.0 \pm 2.0$	n.s.
2-Year follow-up	$2.4\pm2.2$	$1.8\pm2.0$	0.038
<i>p</i> value	<0.001	<0.001	

All values are given as the mean and the standard deviation

*CVI* conventional instrumentation, *KSS* Knee-Society-Score, *PSI* patient-specific instrumentation, *VAS* visual analog scale for pain

WOMAC (85.7  $\pm$  17.9 vs. 86.7  $\pm$  15.4, respectively) and the OKS (35.9  $\pm$  10.3 vs. 35.8  $\pm$  9.3, respectively).

While the mean postoperative HKA was not significantly different between the groups, the mean deviation from a neutral mechanical alignment was significantly lower in the PSI group (Table 3). Additionally, the accuracy of femoral and tibial component positioning was significantly higher in all planes, except for LFC (Table 3).

More than half of all PSI cases (57 %) reached postoperative HKA of  $180^{\circ} \pm 1^{\circ}$ . Mechanical alignment restoration grouped by degrees of deviation from the targeted neutral axis is presented in Fig. 3.

Further radiological evaluation showed significant reductions of outliers regarding HKA (outlier  $>3^{\circ}$  and  $>5^{\circ}$ ) and 3D-component positioning (Table 4) in the PSI group. All clinical parameter, except ROM, were significantly better in HKA non-outliers compared with HKA-outliers (Table 5).

# Discussion

In this prospective single-center study, the most important findings were that (a) PSI showed significantly superior accuracy in mechanical alignment restoration and 3D-component positioning compared with CVI in primary TKA and (b) clinical outcome was comparable between the two instrumentation groups at early follow-up, whereas KSS, VAS, WOMAC, and OKS were significantly better in the subgroup of knees within  $\pm 3^{\circ}$  of deviation from a neutral mechanical axis compared with outliers.

As patient-specific cutting or pin-positioning blocks are still relatively new, but potentially feasible methods to aid the surgeon in reaching satisfactory component positioning and overall limb alignment, efforts are made to improve accuracy and reliability of such methods. Current studies have found controversial results regarding mechanical alignment with reported outlier rates (deviation  $>3^\circ$ ) from 3 to 49 % [2, 4, 8, 9, 11, 14, 30, 40, 44, 61]. Interestingly, studies using even the same PSI technique reported inconsistent results ranging from 7 to 45 % [16, 37, 47, 61]. While on one hand the outlier rate in one of the only two studies evaluating the same PSI system as in the present study was with 12 % [29] comparable with our findings, the other study [16] with a 37 % outlier rate was not. A possible reason for such variances might be a considerable difference in sample size (291-23, respectively). Furthermore, the authors [16] reported that according to intra-operative navigation control and postoperative X-ray assessment. single component measurements for the coronal plane

Table 3 Radiological outcome between conventional (CVI) versus PSI after total knee arthroplasty

	CVI group <sup>a</sup> $(n = 108)$	PSI group <sup>b</sup> $(n = 114)$	<i>p</i> value
HKA (°)			
Preoperative	$176.4 \pm 6.3$	$175.6 \pm 6.4$	n.s.
Postoperative	$180.0 \pm 2.8$	$179.6 \pm 2.0$	n.s.
<i>p</i> value	<0.001	< 0.001	
Preoperative varus knees (°)	$173.7 \pm 4.3$	$172.8 \pm 3.6$	n.s.
Preoperative valgus knees (°)	$184.6 \pm 3.9$	$185.3 \pm 4.1$	n.s.
HKA-deviation from neutral (°)	$2.2 \pm 1.7$	$1.5 \pm 1.4$	< 0.001
Of preoperative varus knees (°)	$2.2 \pm 1.7$	$1.4 \pm 1.4$	0.002
Of preoperative valgus knees (°)	$2.3 \pm 1.7$	$1.6 \pm 1.3$	n.s.
FFC (°)	$91.1 \pm 2.2$	$90.2 \pm 1.5$	< 0.001
FFC deviation from 90° (°)	$2.0 \pm 1.4$	$1.1 \pm 0.9$	< 0.001
FTC (°)	$88.8 \pm 1.7$	$89.6 \pm 1.4$	0.001
FTC deviation from 90° (°)	$1.5 \pm 1.4$	$1.2 \pm 0.9$	0.019
LFC (°)	$88.5 \pm 2.5$	$86.7 \pm 2.7$	< 0.001
LFC deviation from 86°–90° (°)	$0.7 \pm 1.2$	$0.8 \pm 1.5$	n.s.
LTC (°)	$85.2 \pm 2.8$	$86.2 \pm 2.3$	0.004
LTC deviation from 84°–90° (°)	$0.6 \pm 1.2$	$0.2 \pm 0.7$	0.002
FCR deviation from 0° (°)	$2.3 \pm 1.5$	$1.7 \pm 0.9$	0.046

All values are given as the mean and the standard deviation

*CVI* conventional instrumentation, *FCR* femoral component rotation, *FFC* frontal femoral component angle, *FTC* frontal tibial component angle, *HKA* hip-knee-ankle angle, *LFC* lateral femoral component angle, *LTC* lateral tibial component angle, *PSI* patient-specific instrumentation

<sup>a</sup> The CVI group consisted of 81 varus and 27 valgus knees. FCR was evaluated in a subgroup of 25 patients in each group

<sup>b</sup> The PSI group consisted of 89 varus and 25 valgus knees. FCR was evaluated in a subgroup of 25 patients in each group



Fig. 3 Hip-knee-ankle angle (HKA) grouped by degrees of deviation from the targeted neutral axis after total knee arthroplasty with conventional (CVI) and PSI

 Table 4
 Comparison of outliers between conventional (CVI) versus

 PSI after total knee arthroplasty

	CVI group	PSI group	p value
HKA-outlier (<177°; >183°)	22.2 % (24/108)	9.6 % (11/114)	0.010
HKA-outlier (<175°; >185°)	7.4 % (8/108)	1.8 % (2/114)	0.042
FFC outlier (<88°; >92°)	42.6 % (46/108)	12.3 % (14/114)	<0.001
FTC outlier (<88°; >92°)	28.7 % (31/10)	10.5 % (12/114)	0.001
LFC (<84°; >92°)	14.8 % (16/108)	6.1 % (7/114)	0.034
LTC (<82°; >92°)	14.8 % (16/108)	3.5 % (4/114)	0.003
FCR ( $<-2^{\circ}; >2^{\circ}$ )	32.0 % (8/25)	4.0 % (1/25)	0.010

*CVI* conventional instrumentation, *PSI* patient-specific instrumentation, *HKA* hip-knee-ankle angle, *FFC* frontal femoral component angle, *FTC* frontal tibial component angle, *LFC* lateral femoral component angle, *LTC* lateral tibial component angle, *FCR* femoral component rotation showed satisfactory results, whereas the overall mechanical alignment was unsatisfactory. Despite the fact that we also performed long-leg radiographs for early evaluation after surgery, which Ensini et al. [16] blamed to be a possible reason for malalignment, we are not able to confirm their findings, since we detected a mean of less than 2° deviations from targeted component position in all planes as well as in HKA. Although Koch et al. [29] did not include a CVI group, PSI results of 291 patients were comparable with the present HKA-outliers (12 vs 10 %, respectively). However, the overall mechanical alignment outlier rate of our PSI group is among the lowest currently reported.

Victor et al. [61] recently reported in a randomized controlled trial no improvements regarding accuracy of mechanical axis restoration and three-planar component positioning with four different PSI systems compared with CVI. These findings are in contrast to the results of the present study. Possible reasons for such differences may include the fact that four different PSI technologies with only 16 patients in each group were evaluated, from which a total of 22 % PSI cases were considered as outliers because intra-operative navigation control measurement exceeded alignment targets. Furthermore, it is difficult to compare our data with values from a combination of intraoperative navigation and postoperative full leg radiograph data. It is well accepted that accurate alignment measurements with navigation are superior to CVI [19, 58], but a recent meta-analysis [21] comparing CVI with computerassisted surgery reported a HKA-outlier rate of 13 % in large population; thus, it is also not warranted that with navigation, surgeons are able to achieve their targets in every single case. Two studies [29, 41] compared their PSI findings with data from meta-analyses of navigation procedures and found no superiority of one or the other technique. However, instead of intra-operative navigation control and possible abandoning PSI, we verified the tibial and femoral cutting block position and cut height with an extramedullary guidance rod and sickle finger, and planned resection was checked with the 3D model. To our experience, a perfect cutting block positioning was only given,

Table 5 Comparison of clinical outcome between non-outliers and outliers of mechanical alignment

	HKA non-outlier ( $\leq 3^{\circ}$ ) ( $n = 187$ )	HKA-outlier (>3°) ( $n = 35$ )	p value
KSS knee* (0–100 points)	$93.2 \pm 9.9$	88.6 ± 16.3	0.027
KSS function* (0-100 points)	$85.8 \pm 16.7$	$74.0 \pm 24.3$	< 0.001
Range of motion* (°)	$117.2 \pm 11.7$	$114.4 \pm 13.0$	n.s.
VAS pain* (0–10 points)	$1.9 \pm 1.9$	$3.0 \pm 2.9$	0.003
WOMAC score* (0-100 points)	$87.8 \pm 14.5$	$77.4 \pm 23.5$	0.001
Oxford-Knee-score* (0-48 points)	$36.8 \pm 9.2$	$30.9 \pm 11.4$	0.001

KSS Knee-Society-Score, VAS visual analog scale for pain, WOMAC the Western Ontario and McMaster Universities Osteoarthritis Index

\* The values are given as the mean and the standard deviation

if all remaining cartilage was precisely removed from foot print areas. Indeed, we found similar HKA alignment and favorable 3D component accuracy with PSI compared with a computer-assisted surgery group of Hetaimish et al. [21].

The reasons for the heterogeneity of reported accuracy in contemporary PSI systems are yet not clear. Nonetheless, published studies mainly focus on PSI systems relying on MRI-based manufacturing of cutting blocks [4, 8, 35, 43, 61], whereas reports of CT-based PSI are relatively rare [29, 61]. In general, MRI may be better in defining cartilage surface, and CT scans have the advantage of a distinct visualization of femoral and tibial bone-cartilage interface. Therefore, degeneration and mechanical properties of the cartilage surface, especially in severe osteoarthritis, can alter correct cutting block or pin-guide placement. Such imprecision can easily be avoided by relying on bony landmarks [62, 65]. At the initial phase of the present study, we decided to use CT scans as it was considered to be the ultimate precision tool in measuring lower limb alignment [10]. A recently published randomized clinical trial reported slightly better accuracy with MRI-based compared with CT-based PSI [47], whereas another randomized clinical trial comparing three different MRI- and one CT-based PSI system showed inconsistent results [61]. Further investigations comparing a CT-based with an MRI-based PSI version of the same system would be of interest, but was beyond the scope of the current study.

To our knowledge, we are the first to present clinical data 2 years after TKA using PSI. Few clinical outcome studies comparing PSI and CVI in TKA have shown heterogeneous results, but follow-up periods were less than one year [48, 64, 66, 67]. While Pietsch et al. [48], Woolson et al. [66], and Vundenlickx et al. [64] reported no difference in clinical outcome between PSI and CVI, and Yaffe et al. [67] reported significant improvements with PSI, we detected subtle clinical differences between the instrumentation groups at the 2-year follow-up. Interestingly, we found significant differences between CVI and PSI regarding VAS for pain, but not with the pain-emphasized standardized WOMAC score. Both scores are patient generated and therefore influenced by various subjective conditions (e.g., depression) and expectations [23]; thus, it remains unclear how to interpret such differences. The other significant difference was detected with KSS function, which is known to have a poor correlation with the function part of the WOMAC score [31, 59]. However, it is still not clear if the two detected as significant differences are of clinical relevance; therefore, further long-term clinical investigations are required.

The influence of limb alignment on clinical outcome is not yet clear. Various studies showed an association between malalignment and decreased clinical outcome [12, 27, 33], whereas more recent studies suggested no negative effect of residual deformity on clinical results [36, 38, 60]. In contrast to the weak clinical differences between the two instrumentation cohorts of our study, a comparison of HKA-outliers and non-outliers (assuming a  $\pm 3^{\circ}$  target) showed significantly better clinical outcome in the group of non-outliers. These findings not only confirm the importance of accurate limb alignment and component positioning, but also that a combination of clinical and radiological assessment is of additional value.

The present study has some limitations. One limitation of the study is that it was not randomized. However, the two consecutive groups were not significantly different regarding demographics and preoperative limb alignment. A further possible influencing factor is that we used either medial or lateral parapatellar surgical approach according to varus or valgus, which might influence clinical and radiological outcome, but the deformity distribution was not significantly different in both groups. Nonetheless, to our knowledge, the current study is the first reporting on clinical outcome of PSI versus CVI in primary mobile-bearing TKA with a follow-up of 2 years. Furthermore, it is among the largest studies currently available that compared radiological outcome between PSI and CVI in primary TKA.

# Conclusion

The importance of this study lies in the findings that CTbased PSI compared with CVI improved accuracy of alignment restoration and 3D-component positioning in primary TKA. Such a reduction could be a feasible way to further improve patients' outcome and satisfaction in TKA. Although clinical outcome was similar in both instrumentation groups at early follow-up, significantly inferior outcome was detected in the subgroup of HKA-outliers. However, further long-term studies are necessary to evaluate clinical and radiological outcome as well as implant survival after TKA using PSI.

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**Conflict of interest** The TKA system GMK<sup>®</sup> Primary was designed by Medacta International S.A., Castel San Pietro, Switzerland, in cooperation with the senior author, who will receive royalties for his contribution regarding the design of the implant. XX is a consultant for Medacta. However, Medacta had no influence on study design, data collection, interpretation of the results, or the writing of the final article. There was no external funding source for this study.

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